

Tailoring Brain Stimulation to the Nature of Rehabilitative Therapies in Stroke

A Conceptual Framework Based on their Unique Mechanisms of Recovery



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KEYWORDS

- Stroke • Unilateral therapy • Bilateral therapy • Noninvasive brain stimulation
- Transcranial direct current stimulation • Repetitive transcranial magnetic stimulation
- Upper limb • Motor impairment

KEY POINTS

- Noninvasive brain stimulation is typically paired with unilateral therapies of the upper limb.
- Many recent clinical trials have failed to augment rehabilitative outcomes, especially for patients with greater motor impairments.
- Bilateral therapies may offer a more feasible and neurophysiologic advantage over unilateral therapy to augment rehabilitative outcomes for patients with greater motor impairments.
- Based on mechanisms of recovery, this article discusses how to create noninvasive brain stimulation paradigms that are tailored to the individual type of therapy (unilateral or bilateral) across varying degree of impairments.

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INTRODUCTION

Stroke is a leading cause of long-term adult disability. Although current rehabilitation strategies carry promise, gains are modest where approximately 60% to 80% of survivors continue to experience motor impairments of the upper limb well into the chronic phase of recovery.^{1–3} One reason for the modest recovery of upper-limb function is the diminishing access to rehabilitation, where therapists are required to administer best practice in a limited number of sessions. To address this limitation, current research emphasizes the need for maximizing and accelerating outcomes of rehabilitation within a limited amount of time.

To augment rehabilitative benefits, use of noninvasive brain stimulation (NIBS) has become a popular topic of research. Specifically, NIBS has the potential to augment mechanisms of plasticity that underlie rehabilitation-related recovery. The most commonly used forms of NIBS in research include repetitive transcranial magnetic stimulation (rTMS) and transcranial direct current stimulation (tDCS). rTMS operates by using electromagnetic induction, wherein an insulated coiled wire is placed on the scalp. Then, at varying frequencies, the coil produces a brief and strong alternating current that induces a perpendicular spatially focused magnetic field. The magnetic field induces current, which passes unimpeded through the skull, resulting in depolarization of neurons in superficial cortices.⁴ High-frequency pulses (≥ 5 Hz) are used to facilitate excitability of the targeted cortices,⁵ whereas low-frequency pulses (< 1 Hz) inhibit excitability of the underlying cortices.⁶ Unlike rTMS, tDCS applies current directly to the targeted regions and has emerged as a popular NIBS approach because it is simple and easy to use in conjunction with physical and occupational therapy.^{7,8} Using a constant current stimulator, surface electrodes placed in saline-soaked sponges deliver low-levels of direct current (0–4 mA) to the scalp and create changes in cortical excitability.⁹ Early animal studies have shown that tDCS modulates neuronal membrane potentials in the cortices, such that anodal tDCS depolarizes membrane potentials and cathodal tDCS hyperpolarizes membrane potentials.¹⁰ As such, anodal tDCS is typically considered excitatory for the targeted region, whereas cathodal tDCS is considered inhibitory. Although the exact mechanisms are unclear, a similar directional change in excitability has been achieved in humans. Nitché and Paulus¹¹ have shown that anodal tDCS increases excitability and cathodal tDCS decreases cortical excitability. Based on pharmacologic studies, the likely mechanism in humans involves up-regulation of *N*-methyl-D-aspartate receptor activity¹² and modulation of γ -aminobutyric acid (GABA)ergic neuronal activation.¹³ Thus, tDCS modulates excitability and spontaneous firing rate of neurons.

The primary application of NIBS approaches in rehabilitation has involved their pairing with unilateral upper-limb therapies. Such therapies focus on intensively retraining the paretic limb and restraining or otherwise discouraging movement of the nonparetic limb. Examples include constraint-induced movement therapy, unilateral task-oriented practice, or learning involving only the paretic limb, among several others.^{14–18} NIBS approaches are applied before therapy (rTMS) or during therapy (tDCS).

Despite promising early studies,^{19,20} NIBS has shown somewhat limited effects to augment rehabilitative outcomes of the unilateral upper limb in more recent and larger clinical trials.^{15,16,21–25} Hence, its use remains for the most part investigational. In trying to understand the failures, it seems that the benefits of NIBS plus therapy are modest, and vary considerably from patient-to-patient, failing especially in patients with greater motor impairments.^{15,26} Thus, this article addresses important lingering questions that may help devise the best combinations of NIBS with rehabilitative therapies. Are mechanisms that NIBS seeks to entrain in its pairing with unilateral therapy

generalizable across patients in all ranges of impairment, or do these mechanisms fail across patients with greater motor impairments? In such cases, are therapies targeting alternate mechanisms better suited for the more impaired instead?

Several groups have recently suggested the importance of bilateral behavioral therapies as alternates to unilateral upper-limb therapies, including bilateral arm training with rhythmic auditory cueing (BATRAC),²⁷ bilateral isokinematic training,²⁸ active-passive bilateral training (APBT), and contralaterally controlled functional electrical stimulation (CCFES).²⁹ Even though there is no direct evidence concluding whether they are better than unilateral therapies across certain ranges of severity, it is generally considered that they likely could be more efficacious for patients with greater motor impairments,^{30–32} because many of the previously mentioned therapies enable the nonparetic limb to drive movement of the paretic limb. However, there is limited understanding of what mechanisms underlie bilateral therapies, which is why there is lack of discussion on how to pair NIBS with bilateral therapies. In contrast, the mechanisms underlying unilateral therapies are better understood, which is why there is considerable evidence discussing how to apply NIBS to affect outcomes of unilateral therapies. The aim of this article is to (1) compare possible mechanisms of recovery that may be engaged by unilateral and bilateral therapies, (2) explain potentially how these mechanisms may vary across ranges of damage and impairment, and (3) present a theoretic framework for how to create NIBS paradigms that are tailored to distinctly augment bilateral and unilateral therapies.

MECHANISMS OF RECOVERY UNDERLYING UNILATERAL THERAPY

Typically, coordination between limbs requires modulating motor overflow, where motor overflow refers to facilitation from the “moving” cortices to the opposing “resting” hemisphere. During unilateral movement of a limb, mirror movements can occur in the opposite resting limb if motor overflow is not regulated. Interhemispheric interactions conducted via transcallosal pathways between both hemispheres help regulate overflow. Specifically, the hemisphere contralateral to the moving limb imposes an inhibitory influence on the ipsilateral hemisphere, whereas the ipsilateral hemisphere relaxes its counterinhibition to allow for a purely unilateral movement.^{33,34}

Following stroke, however, the mechanism of regulating motor overflow is disrupted, resulting in a series of events that constitutes what is commonly referred to as the interhemispheric competition model.^{35–37} Based on this model, during unilateral movement of the paretic limb, the affected hemisphere weakly inhibits the unaffected hemisphere to regulate overflow (**Fig. 1**).^{38–40} In turn, the “disinhibited” unaffected hemisphere overly inhibits the affected hemisphere, further weakening its excitability and the drive to move the paretic limb.⁴¹ Such an imbalance of mutual inhibition presumably exacerbates as patients rely on using their nonparetic limb at the cost of the weak paretic limb.⁴² Therefore, the typical recommendation based on the interhemispheric competition model is to unilaterally retrain the paretic limb but restrain or discourage movements of the nonparetic limb.^{43–45} By intensively retraining the paretic limb, it is believed the weak affected hemisphere is facilitated, and effectively counters inhibition from the unaffected hemisphere, promoting gains in recovery of the upper limb.

COMBINING NONINVASIVE BRAIN STIMULATION WITH UNILATERAL THERAPY BASED ON THEORY OF UNDERLYING MECHANISMS

In accordance with the interhemispheric competition model, present-day NIBS approaches aim to upregulate excitability of the affected hemisphere but inhibit that of

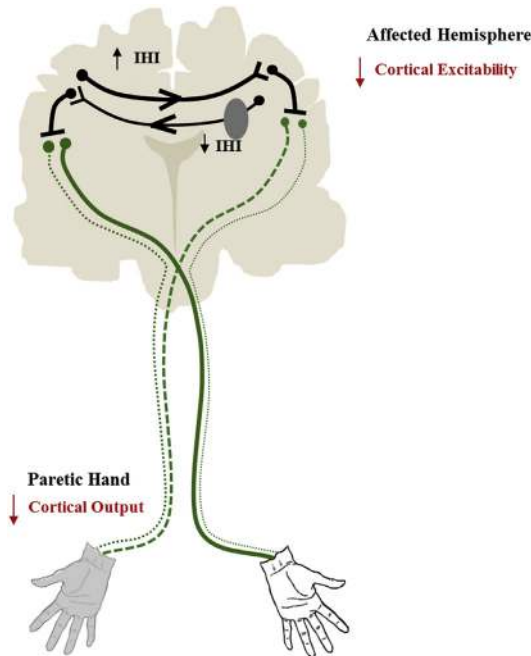


Fig. 1. Interhemispheric competition model with chronic stroke. The lesion reduces interhemispheric inhibition (IHI) exerted by the effect on the unaffected hemisphere. In turn, the disinhibited unaffected hemisphere generates exaggerated inhibition on the affected hemisphere, which reduces excitability and cortical drive to the paretic limb. Dark circle represents the lesion.

the unaffected hemisphere to enhance rehabilitative outcomes. Toward this end, multiple research groups have used high-frequency rTMS or anodal tDCS to excite the affected hemisphere or low-frequency rTMS or cathodal tDCS to inhibit the unaffected hemisphere (Fig. 2; for a full review see Hoyer and Celnik⁴⁶ or Sandrini and Cohen⁴⁷). In either hemisphere, the most common target is the primary motor cortex (M1), because evidence suggests its adaptive plasticity is intimately associated with paretic upper-limb recovery.^{48–50}

LIMITATIONS OF UNILATERAL THERAPIES AND ASSOCIATED NONINVASIVE BRAIN STIMULATION APPROACHES

Larger clinical trials have had limited success when replicating the early promise of pairing NIBS with unilateral therapies.^{15,16,22–25,51} One possible reason for the disappointing results is that the groups were less homogenous and included patients with a wider range of impairment than in earlier smaller studies. Previous studies have discussed that pairing NIBS with unilateral therapy is less effective for the more impaired chronic stroke patients.^{15,26} An important question to consider is whether the model of interhemispheric competition informing unilateral therapies and present-day NIBS approaches in the chronic stroke population is applicable across patients with greater severity. We describe three major reasons for why exciting the affected hemisphere and/or inhibiting the unaffected M1 may generalize poorly across patients with greater severity: (1) heterogeneity of stroke population, (2) extent

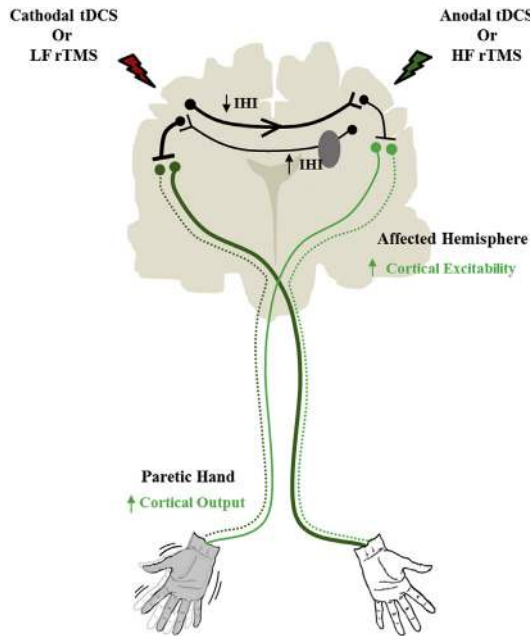


Fig. 2. Current NIBS approach. Anodal tDCS or high-frequency (HF) rTMS targets the affected hemisphere to increase the excitability of the affected hemisphere and cortical output to the paretic hand. Cathodal tDCS or low-frequency (LF) rTMS is applied to unaffected hemisphere to reduce the inhibition imposed on the affected hemisphere. Dark circle represents the lesion.

of damage in the affected hemisphere, and (3) the influence of the unaffected hemisphere.

Stroke Population Heterogeneity

Within the stroke population, such factors as age, location and profile of lesion, and comorbidities all show high variation.⁵² Furthermore, many of these factors also contribute to the large variability in overall severity of the motor deficit, with some patients having substantial amounts of movement and others having limited movement in the paretic upper limb. Applying unilateral therapy to patients with limited movement can inherently be challenging. Specifically, because of their inability to use their paretic limb in task-based therapies, severely impaired patients are generally unable to realize the maximum benefits from unilateral therapies, which may explain why they show greater inconsistencies in benefits of NIBS. Most of these patients are unable to meet the minimal movement criteria for participation in unilateral rehabilitation, where often participants are required to have at least 20° of wrist extension and 10° extension of at least two fingers.⁵³ When severely impaired patients are included in trials, they do not show the same recovery as the less impaired, suggesting that unilateral behavioral therapies may be less successful and feasible for this population.^{31,54,55} Therefore, current NIBS approaches combined with unilateral therapies generalize poorly across the more impaired patients because the fundamental therapy itself is inconsistently effective for this population.

Damage in the Affected Hemisphere

When patients experience hemiparesis following stroke, those with subcortical lesions typically have damage to the corticospinal tracts. The corticospinal tract originates from the primary and premotor cortices where the descending pathways synapse with lower motor neurons at the level of the spinal cord to execute volitional movements. It has previously been shown with diffusion tensor imaging that patients with poor integrity of corticospinal tracts following stroke exhibit more severe motor impairments.^{56–59} Thus, it is possible that patients, especially those with severe motor impairments, do not have adequate residual corticospinal pathways that can be excited in the affected hemisphere with unilateral therapies or with current NIBS approaches. Hence, they fail to benefit from modulation of interhemispheric mechanisms of recovery for the paretic limb.^{26,60}

Influence of the Unaffected Hemisphere

Several groups,^{58,61–64} including our own,⁵⁷ have demonstrated that the unaffected hemisphere is not always inhibitory to the affected hemisphere as traditionally believed. Rather, it can mediate recovery when substrates in the affected hemisphere are damaged considerably and patients experience greater severity of impairment.³⁶ Machado and colleagues⁶⁵ show that following hemispherectomy, the unaffected hemisphere in rodent models assumes the role of the affected hemisphere, suggesting it becomes critical for recovery. In fact, rodents with large lesions experience a decline in motor function when the unaffected hemisphere is anesthetized.⁶¹ As such, the unaffected hemisphere may provide an adaptive role through ipsilateral pathways originating from the unaffected hemisphere and innervating lower motor neurons devoted to the paretic limb. Carmel and colleagues⁶⁶ have recently demonstrated in a rodent model that electrical stimulation applied to facilitate the unaffected hemisphere promotes recovery of skilled forelimb behavior through ipsilateral pathways. Furthermore, Bachmann and colleagues⁶⁷ demonstrated in a mouse model that unilateral strokes induces axonal sprouting from the unaffected hemisphere at the level of the brainstem–spinal cord connections, with the possibility to gain control over the affected limb.

The potential adaptive role of the unaffected hemisphere in humans also aligns with these animal studies. For example, when TMS is applied transiently to disrupt the unaffected premotor cortex, patients with greater impairments experience greatest disruption in motor performance of the paretic hand, suggesting that with greater impairment, the likely role of the unaffected cortices becomes more relevant.⁶⁴ Furthermore, if NIBS is applied to inhibit the unaffected hemisphere, patients with greater impairments experience a transient decline in upper-limb motor function, suggesting that with greater impairment, unaffected cortices likely offer an adaptive potential for recovery.⁶⁸ These studies suggest that the role of the unaffected hemisphere is expressed more so with greater impairment and deficit, where its influence can be considered more adaptive than what is known typically. Although animal studies facilitating the unaffected hemisphere in models of greater damage⁶⁶ have recently supported these new views by demonstrating a causal adaptive role of the unaffected hemisphere in chronic recovery, direct evidence as to the total contribution of the unaffected hemisphere in humans remains to be seen.

The heterogeneity of the stroke population, extent of damage of the affected hemisphere, and the influence of the unaffected hemisphere may explain the shortcomings of unilateral therapies and the inconsistencies of the resultant NIBS studies. The generalizability of the theory of interhemispheric competition as a global mechanism

of motor recovery following stroke thus becomes questionable. By emphasizing a single mechanism we risk creating augmentative NIBS approaches that lack flexibility to consistently serve the spectrum of stroke patients. In the same vein, we are likely to miss the advantages of potentially high-yielding therapies, such as bilateral behavioral paradigms, that might also promote recovery.

BILATERAL THERAPY AS AN ALTERNATIVE APPROACH

Bilateral approaches differ from unilateral therapies because they require moving both limbs simultaneously, either independently or in a linked manner. For example, bilateral isokinematic training²⁸ requires patients to move both limbs, but actions of one are not dependent or controlled by actions of the other. In contrast, Stinear and Byblow's⁶⁹ APBT, Whittall and colleagues's²⁷ BATRAC, and Knutson and colleagues's²⁹ CCFES link movements of both limbs. Using external instrumentation, such as mechanical fixations or electrical stimulation, the nonparetic limb drives the movement of the paretic limb.

Regardless of the type, bilateral therapies may provide a more feasible alternative to unilateral therapies. Because patients with severe impairments are typically unable to participate in unilateral therapies, bilateral therapies, such as APBT, BATRAC, and CCFES, where movement of the nonparetic limb drives movement of the paretic limb, could potentially provide all patients an opportunity to be involved and benefit from rehabilitation.

Although bilateral therapies may be more feasible, the important question is whether they are more efficacious than unilateral therapies. Overall, results are equivocal and seem to depend on at least the severity of motor impairment and the nature of clinical outcome of interest. For example, in a recent systematic review, van Delden and colleagues³¹ concluded that bilateral therapies are as effective as unilateral therapies, but unilateral therapies still offered a slight advantage for functional independence and daily use of paretic hand across patients with mild-to-moderate impairment of the distal upper limb. In contrast, McCombe Waller and Whittall³⁰ argue that bilateral therapies involving repetitive reaching, as in BATRAC, offer an advantage for patients with moderate-to-severe impairments, at least in terms of proximal strength. Whether unilateral therapies improve independence and use of hand in daily life or bilateral therapies serve as a useful alternative for proximal function, their effectiveness can be best contrasted when the effect of initial impairment is balanced and the clinical goal is carefully considered.

Mechanisms of Bilateral Movement in Chronic Stroke

If indeed bilateral therapies afford greater advantage than unilateral therapies across the moderate-to-severely impaired patients, then this would suggest that their underlying mechanisms are more resilient in the presence of greater damage. Understanding these mechanisms of recovery could help derive a model that supplements the classical theory of interhemispheric competition. Here, we summarize evidence of potential mechanisms underlying bilateral therapies.

First, whether passive or active, bilateral movements could engage both hemispheres. One clear advantage would be that the unaffected hemisphere, now with evidence pointing to its adaptive and compensatory role for the more impaired patients, would naturally become engaged. Recruiting the unaffected hemisphere could indirectly facilitate the weak affected hemisphere because by symmetrically moving both limbs for a common purpose, both hemispheres become coupled.^{28,70} As a result of coupling, Mudie and Matyas²⁸ explain, the unaffected hemisphere may offer

a template of motor network recruitment to the affected hemisphere, allowing the paretic limb to learn from the nonparetic limb. This may be particularly necessary in more impaired patients where the damaged hemisphere has insufficient cortical-corticospinal resources to affect its own movement plans.

However, what is the evidence that a template could be uniquely elicited in bilateral movement? Studies with functional MRI (fMRI) show that bilateral movements elicit unique and greater activation of bilateral primary sensorimotor, premotor, and supplementary motor cortices in comparison with unilateral movements,⁷¹ and that these distinctions amplify with therapy.²⁷ Patients who show the greatest recovery with BATRAC exhibit the highest gains in fMRI activation in the unaffected hemisphere, especially the unaffected premotor cortex, whereas patients who experience greater functional recovery with unilateral therapy exhibit greater activation of the premotor cortex of the affected hemisphere. Therefore, fMRI activation demonstrates that substrates recruited in bilateral movement are extensive and bihemispheric, compared with those recruited in unilateral movement.

Still, fMRI evidence alone may not be able to verify that a template of learning indeed transfers from one hemisphere to the other during bilateral movement. Studies that assess the neural basis of motor planning or functional and effective connectivity between hemispheres are needed for confirmation. As an example, TMS could reveal the neurophysiologic substrates underlying a transfer. Following stroke, one conceivable outlet for coupling and transfer of learning could involve mutual disinhibition of both hemispheres (Fig. 3).^{72–75} Bilateral movements are in a unique position to potentiate disinhibition unlike unilateral movements because bilateral symmetric movements are considered natural and the default state of interlimb coordination.^{28,70} Therefore, with bilateral synchronous movements, there is a decrease in intracortical inhibition within M1 and interhemispheric inhibition between M1s as demonstrated with TMS.^{32,69,76} Release of inhibition could facilitate excitability of corticospinal output from the affected M1 and help restore the balance of mutual interhemispheric

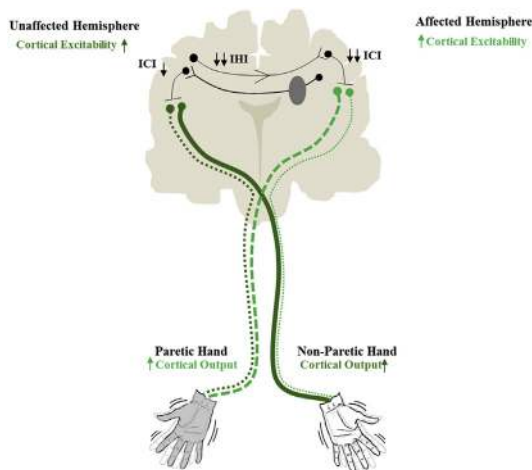


Fig. 3. Mechanisms of bilateral therapy in chronic stroke. Symmetric movements of the paretic and nonparetic limb may result in reduced intracortical inhibition (ICI) of the affected and unaffected hemisphere, and reduced interhemispheric inhibition (IHI) imposed on the affected hemisphere resulting in overall disinhibition of the corticomotor networks. Dark circle represents the lesion.

inhibition. Thus, it is possible that synchronous somatosensory feedback in bilateral motion, and a single set of motor commands linking bimanual movements may help upper limbs to become functionally coupled, and both hemispheres to release their inhibition on one another to allow transfer and exchange of learning.

Pathways Subserving Potential Benefits of Bilateral Therapies

Ultimately, whether it is recruitment of the unaffected hemisphere or transfer of learning via global disinhibition across hemispheres, how are these neurophysiologic effects of bilateral movements ultimately conveyed to affect the recovery of the paretic upper limb? We summarize evidence of potential pathways next ([Fig. 4](#)).

Spared corticomotor neuronal pool of the affected hemisphere

Sparing of corticomotor pathways in the affected hemisphere to the paretic limb depends on the severity of stroke. However, following stroke, cortical plasticity occurs such that higher motor areas (eg, the premotor cortex) can assume the role of the M1. In fact, higher-order areas have been shown to express plasticity in recovery with greater damage and impairment^{77,78} and are important contributors during bilateral arm training and movements.^{27,71} Thus, the release of interhemispheric and intracortical inhibition that occurs during symmetric bilateral movements may increase the motor overflow from the unaffected, “moving” cortices to the affected cortices partnering in bilateral movement.^{27,32,70,79} It has previously been suggested that patients who exhibit greater motor overflow to the affected hemisphere had better motor function than those without motor overflow.⁸⁰ Thus, symmetric bilateral movements could

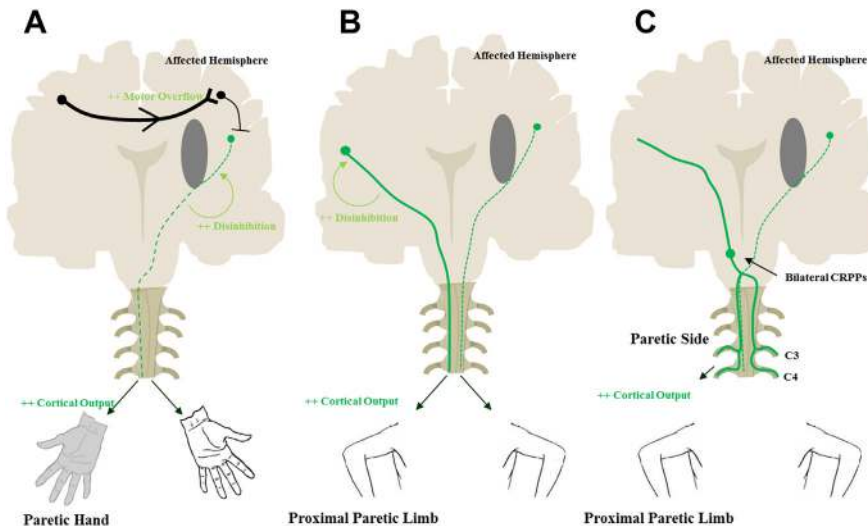


Fig. 4. Mechanisms of recovery following bilateral movement. (A) The affected hemisphere excitability is facilitated via release of interhemispheric and intracortical inhibition, and motor overflow from the unaffected hemisphere. (B) Direct ipsilateral pathways originating from the premotor cortex are thought to be facilitated following the disinhibition that occurs because of symmetric bilateral movement. The direct ipsilateral pathways synapse directly to alpha motor neurons to facilitate increased cortical output to the proximal paretic limb. (C) Indirect ipsilateral pathways (cortico-reticulo-proprio-spinal [CCRP]) synapse at the C3/C4 vertebrae to augment proprio-spinal neurons devoted to the proximal paretic limb.⁸² Dark circle represents the lesion.

be powerful triggers to facilitate excitability of spared pathways originating from higher-order areas more so than unilateral movement for patients with greater motor impairment. Disinhibition and heightened excitability may help the affected hemisphere preserve as much function as possible to the affected areas (see [Fig. 4A](#)).²⁸

Direct and indirect ipsilateral corticospinal pathways from the unaffected hemisphere

Approximately 10% to 15% of the corticospinal fibers originating from each hemisphere, primarily from the premotor cortex,⁸¹ remain uncrossed and project directly to motor neurons devoted to the ipsilateral upper limb.⁸² Several groups have noted unmasking of such ipsilateral pathways in stroke, suggesting that the ipsilateral output from the unaffected hemisphere could be beneficial for recovery.^{58,64,65,82,83} Disinhibition during bilateral movements could cause ipsilateral pathways from the unaffected hemisphere to become unmasked and serve as much needed corticomotor output to the paretic limb (see [Fig. 4B](#)). Furthermore, aside from the direct ipsilateral pathways, nonhuman primate studies reveal that indirect ipsilateral pathways from the unaffected hemisphere are also capable of interacting with motor neurons to the paretic limb.⁸² Mudie and Matyas²⁸ cite reticulospinal and the rubrospinal pathways as candidates to affect recovery of especially the proximal upper limb. More recently, Bradnam and colleagues⁸² proposed that because cortico-reticulo-proprio-spinal pathways originating from the unaffected hemisphere terminate bilaterally on proprio-spinal neurons at the C3/C4 level of the spinal cord, the cortico-reticulo-proprio-spinal tract could theoretically also significantly modulate movement of the affected limb, especially in patients who have limited sparing of the corticospinal tract (see [Fig. 4C](#)).

Importance of Bilateral Therapy for Patients with Greater Impairment

Based on the presented possible mechanisms and pathways, it is conceivable that bilateral therapies could be more efficacious and feasible than unilateral therapies for the more impaired patients. Because patients with greater impairments are believed to recruit the unaffected hemisphere in recovery, performance of bilateral movements may provide an adaptive advantage. With greater coupling and mutual disinhibition, the unaffected hemisphere may strongly affect intracortical and corticospinal excitability of the affected hemisphere in patients who otherwise suffer from substantial damage. Furthermore, mutual disinhibition may allow the unaffected hemisphere to provide an appropriate template of movement to the affected hemisphere. It may help disinhibit “latent but existing” pathways, such as ipsilateral direct and indirect, originating from the unaffected hemisphere, which further promote motor output to the paretic limb, especially the proximal segments. Finally, disinhibition may help recruit affected and unaffected premotor cortices, importance of which we have discussed especially in the context of recovery of proximal function following stroke, a goal that is more reasonable to achieve in the severely impaired.²⁵

NONINVASIVE BRAIN STIMULATION APPROACHES DURING BILATERAL THERAPY

The framework we have summarized regarding mechanisms of bilateral therapies could supply a basis for creating augmentative NIBS approaches. Bradnam and colleagues⁸² previously suggested that because of the potential impact of the indirect ipsilateral corticospinal pathways, one alternative NIBS approach would be to facilitate the unaffected hemisphere to improve paretic upper-limb function. NIBS has typically been used to facilitate the affected hemisphere and inhibit the unaffected hemisphere (see [Fig. 2](#)). However, if NIBS was applied in the same way in conjunction with bilateral therapy as it is with unilateral therapy, we risk either negating the neuro-physiologic benefit of bilateral therapy, or creating the possibility of an even greater

deficit in motor function depending on the availability of the patients' motor substrates in the affected hemisphere.^{68,82,84}

It is reasonable to suggest that facilitating the unaffected and the affected hemisphere together could result in an accelerative advantage when applied in conjunction with bilateral therapy because it would mimic the involvement of both hemispheres during bilateral therapy. Another compelling approach could involve recruiting the supportive role of the premotor cortex of the unaffected hemisphere in patients with greater motor impairments. When TMS is transiently applied to virtually inactivate the premotor cortex of the unaffected hemisphere, patients with greater impairments experience a greater disruption in motor performance of the paretic hand.⁶⁴ Furthermore, during bilateral movement there is greater activation of the unaffected premotor regions,⁷¹ where following therapy there is reorganization that occurs especially in the premotor cortex.²⁷ Therefore, by engaging the unaffected premotor cortex with anodal tDCS or high-frequency rTMS, it is plausible to suggest that greater facilitation of the direct/indirect ipsilateral corticospinal and brainstem-mediated pathways and motor overflow to the affected hemisphere would occur.

Still, regardless of the NIBS approach, careful consideration has to be taken based on the patient's individual level of impairment.⁸² Current evidence suggests patients with severe motor impairments would theoretically benefit from unaffected hemisphere excitation, whereas the mildly impaired patients may benefit to a greater degree by suppressing the unaffected hemisphere excitability in favor of the inter-hemispheric competition model. Still, it remains to be seen whether greater excitation of the contralesional hemisphere in severely impaired patients has an adaptive role for recovery, as indicated by a study in an animal model.⁶⁶ Future studies are needed to investigate the two approaches to compare their efficacy across varying degrees of impairment.

SUMMARY

This article discusses early evidence that bilateral therapy may be feasible and offer an alternative therapeutic advantage to unilateral therapy at least for patients with greater motor impairments. However, to date, no study has demonstrated superiority for either approach. Advances in research have demonstrated a notable shift in how scientists and therapists interpret mechanisms of recovery between patients. Many groups have begun to suggest alternative NIBS protocols and therapies (unilateral or bilateral) that challenge the one-size-fits-all approach. Even though the combinations of NIBS does show promise to maximize/accelerate functional outcomes for patients with chronic stroke, careful consideration should be taken when developing new approaches for delivering NIBS. Because of the literature presented in this review, we argue that perhaps future studies should begin to stratify patients based on individual level of impairment and type of therapy. The goal of stratification will aid in the optimization of resource allocation for current therapists and rehabilitation clinicians. Furthermore, it will take clinicians one step closer to tailoring therapy based on patients' needs.

REFERENCES

1. Broeks JG, Lankhorst GJ, Rumping K, et al. The long-term outcome of arm function after stroke: results of a follow-up study. *Disabil Rehabil* 1999;21(8):357–64.
2. Wilkinson PR, Wolfe CD, Warburton FG, et al. A long-term follow-up of stroke patients. *Stroke* 1997;28(3):507–12.

3. Coupar F, Pollock A, van Wijck F, et al. Simultaneous bilateral training for improving arm function after stroke. *Cochrane Database Syst Rev* 2010;(4):CD006432.
4. Terao Y, Ugawa Y. Basic mechanisms of TMS. *J Clin Neurophysiol* 2002;19(4):322–43.
5. Pascual-Leone A, Valls-Sole J, Wassermann EM, et al. Responses to rapid-rate transcranial magnetic stimulation of the human motor cortex. *Brain* 1994;117(Pt 4):847–58.
6. Chen R, Classen J, Gerloff C, et al. Depression of motor cortex excitability by low-frequency transcranial magnetic stimulation. *Neurology* 1997;48(5):1398–403.
7. Schlaug G, Renga V. Transcranial direct current stimulation: a noninvasive tool to facilitate stroke recovery. *Expert Rev Med devices* 2008;5(6):759–68.
8. Schlaug G, Renga V, Nair D. Transcranial direct current stimulation in stroke recovery. *Arch Neurol* 2008;65(12):1571–6.
9. Wagner T, Fregni F, Fecteau S, et al. Transcranial direct current stimulation: a computer-based human model study. *Neuroimage* 2007;35(3):1113–24.
10. Purpura DP, McMurtry JG. Intracellular activities and evoked potential changes during polarization of motor cortex. *J Neurophysiol* 1965;28:166–85.
11. Nitsche MA, Paulus W. Excitability changes induced in the human motor cortex by weak transcranial direct current stimulation. *J Physiol* 2000;527(Pt 3):633–9.
12. Nitsche MA, Fricke K, Henschke U, et al. Pharmacological modulation of cortical excitability shifts induced by transcranial direct current stimulation in humans. *J Physiol* 2003;553(Pt 1):293–301.
13. Nitsche MA, Liebetanz D, Schlitterlau A, et al. GABAergic modulation of DC stimulation-induced motor cortex excitability shifts in humans. *Eur J Neurosci* 2004;19(10):2720–6.
14. Bolognini N, Vallar G, Casati C, et al. Neurophysiological and behavioral effects of tDCS combined with constraint-induced movement therapy in poststroke patients. *Neurorehabil Neural Repair* 2011;25(9):819–29.
15. Seniow J, Bilik M, Lesniak M, et al. Transcranial magnetic stimulation combined with physiotherapy in rehabilitation of poststroke hemiparesis: a randomized, double-blind, placebo-controlled study. *Neurorehabil Neural Repair* 2012;26(9):1072–9.
16. Talelli P, Wallace A, Dileone M, et al. Theta burst stimulation in the rehabilitation of the upper limb: a semirandomized, placebo-controlled trial in chronic stroke patients. *Neurorehabil Neural Repair* 2012;26(8):976–87.
17. Chang WH, Kim YH, Yoo WK, et al. rTMS with motor training modulates cortico-basal ganglia-thalamocortical circuits in stroke patients. *Restor Neurol Neurosci* 2012;30(3):179–89.
18. Lindenberg R, Renga V, Zhu LL, et al. Bihemispheric brain stimulation facilitates motor recovery in chronic stroke patients. *Neurology* 2010;75(24):2176–84.
19. Hummel FC, Celnik P, Pascual-Leone A, et al. Controversy: noninvasive and invasive cortical stimulation show efficacy in treating stroke patients. *Brain Stimul* 2008;1(4):370–82.
20. Boggio PS, Nunes A, Rigonatti SP, et al. Repeated sessions of noninvasive brain DC stimulation is associated with motor function improvement in stroke patients. *Restor Neurol Neurosci* 2007;25(2):123–9.
21. Plow EB, Arora P, Pline MA, et al. Within-limb somatotopy in primary motor cortex—revealed using fMRI. *Cortex* 2010;46(3):310–21.
22. Hesse S, Waldner A, Mehrholz J, et al. Combined transcranial direct current stimulation and robot-assisted arm training in subacute stroke patients: an exploratory, randomized multicenter trial. *Neurorehabil Neural Repair* 2011;25(9):838–46.

23. Malcolm MP, Triggs WJ, Light KE, et al. Repetitive transcranial magnetic stimulation as an adjunct to constraint-induced therapy: an exploratory randomized controlled trial. *Am J Phys Med Rehabil* 2007;86(9):707–15.
24. Tomasevic L, Zito G, Pasqualetti P, et al. Cortico-muscular coherence as an index of fatigue in multiple sclerosis. *Mult Scler* 2013;19(3):334–43.
25. Plow EB, Cunningham DA, Varnerin N, et al. Rethinking stimulation of the brain in stroke rehabilitation: why higher motor areas might be better alternatives for patients with greater impairments. *Neuroscientist* 2014;21(3):225–40.
26. Emara T, El Nahas N, Elkader HA, et al. MRI can predict the response to therapeutic repetitive transcranial magnetic stimulation (rTMS) in stroke patients. *J Vasc Interv Neurol* 2009;2(2):163–8.
27. Whittall J, Waller SM, Sorkin JD, et al. Bilateral and unilateral arm training improve motor function through differing neuroplastic mechanisms: a single-blinded randomized controlled trial. *Neurorehabil Neural Repair* 2011;25(2):118–29.
28. Mudie MH, Matyas TA. Can simultaneous bilateral movement involve the undamaged hemisphere in reconstruction of neural networks damaged by stroke? *Disabil Rehabil* 2000;22(1–2):23–37.
29. Knutson JS, Harley MY, Hisel TZ, et al. Improving hand function in stroke survivors: a pilot study of contralaterally controlled functional electric stimulation in chronic hemiplegia. *Arch Phys Med Rehabil* 2007;88(4):513–20.
30. McCombe Waller S, Whittall J. Bilateral arm training: why and who benefits? *NeuroRehabilitation* 2008;23(1):29–41.
31. van Delden AE, Peper CE, Beek PJ, et al. Unilateral versus bilateral upper limb exercise therapy after stroke: a systematic review. *J Rehabil Med* 2012;44(2):106–17.
32. Stinear CM, Barber PA, Coxon JP, et al. Priming the motor system enhances the effects of upper limb therapy in chronic stroke. *Brain* 2008;131(Pt 5):1381–90.
33. Giovannelli F, Borgheresi A, Balestrieri F, et al. Modulation of interhemispheric inhibition by volitional motor activity: an ipsilateral silent period study. *J Physiol* 2009;587(Pt 22):5393–410.
34. Bodwell JA, Mahurin RK, Waddle S, et al. Age and features of movement influence motor overflow. *J Am Geriatr Soc* 2003;51(12):1735–9.
35. Nowak DA, Grefkes C, Ameli M, et al. Interhemispheric competition after stroke: brain stimulation to enhance recovery of function of the affected hand. *Neurorehabil Neural Repair* 2009;23(7):641–56.
36. Di Pino G, Pellegrino G, Assenza G, et al. Modulation of brain plasticity in stroke: a novel model for neurorehabilitation. *Nat Rev Neurol* 2014;10(10):597–608.
37. Takeuchi N, Izumi S. Noninvasive brain stimulation for motor recovery after stroke: mechanisms and future views. *Stroke Res Treat* 2012;2012:584727.
38. Boroojerdi B, Diefenbach K, Ferbert A. Transcallosal inhibition in cortical and subcortical cerebral vascular lesions. *J Neurol Sci* 1996;144(1–2):160–70.
39. Shimizu T, Hosaki A, Hino T, et al. Motor cortical disinhibition in the unaffected hemisphere after unilateral cortical stroke. *Brain* 2002;125(Pt 8):1896–907.
40. Ward NS, Cohen LG. Mechanisms underlying recovery of motor function after stroke. *Arch Neurol* 2004;61(12):1844–8.
41. Murase N, Duque J, Mazzocchio R, et al. Influence of interhemispheric interactions on motor function in chronic stroke. *Ann Neurol* 2004;55(3):400–9.
42. Avanzino L, Bassolino M, Pozzo T, et al. Use-dependent hemispheric balance. *J Neurosci* 2011;31(9):3423–8.
43. Page SJ, Levine P. Modified constraint-induced therapy in patients with chronic stroke exhibiting minimal movement ability in the affected arm. *Phys Ther* 2007;87(7):872–8.

44. Wolf SL, Lecraw DE, Barton LA, et al. Forced use of hemiplegic upper extremities to reverse the effect of learned nonuse among chronic stroke and head-injured patients. *Exp Neurol* 1989;104(2):125–32.
45. Taub E, Morris DM. Constraint-induced movement therapy to enhance recovery after stroke. *Curr Atheroscler Rep* 2001;3(4):279–86.
46. Hoyer EH, Celnik PA. Understanding and enhancing motor recovery after stroke using transcranial magnetic stimulation. *Restor Neurol Neurosci* 2011;29(6):395–409.
47. Sandrini M, Cohen LG. Noninvasive brain stimulation in neurorehabilitation. *Handbook Clin Neurol* 2013;116:499–524.
48. Adkins-Muir DL, Jones TA. Cortical electrical stimulation combined with rehabilitative training: enhanced functional recovery and dendritic plasticity following focal cortical ischemia in rats. *Neurol Res* 2003;25(8):780–8.
49. Plautz EJ, Milliken GW, Nudo RJ. Effects of repetitive motor training on movement representations in adult squirrel monkeys: role of use versus learning. *Neurobiol Learn Mem* 2000;74(1):27–55.
50. Bolognini N, Pascual-Leone A, Fregni F. Using non-invasive brain stimulation to augment motor training-induced plasticity. *J Neuroeng Rehabil* 2009;6:8.
51. Plow EB, Carey JR, Nudo RJ, et al. Invasive cortical stimulation to promote recovery of function after stroke: a critical appraisal. *Stroke* 2009;40(5):1926–31.
52. Go AS, Mozaffarian D, Roger VL, et al. Heart disease and stroke statistics–2014 update: a report from the American Heart Association. *Circulation* 2014;129(3):e28–292.
53. Winstein CJ, Miller JP, Blanton S, et al. Methods for a multisite randomized trial to investigate the effect of constraint-induced movement therapy in improving upper extremity function among adults recovering from a cerebrovascular stroke. *Neurorehabil Neural Repair* 2003;17(3):137–52.
54. Bonifer N, Anderson KM. Application of constraint-induced movement therapy for an individual with severe chronic upper-extremity hemiplegia. *Phys Ther* 2003;83(4):384–98.
55. Bonifer NM, Anderson KM, Arciniegas DB. Constraint-induced therapy for moderate chronic upper extremity impairment after stroke. *Brain Inj* 2005;19(5):323–30.
56. Ward NS, Newton JM, Swayne OB, et al. Motor system activation after subcortical stroke depends on corticospinal system integrity. *Brain* 2006;129(Pt 3):809–19.
57. Cunningham DA, Machado A, Janini D, et al. The assessment of inter-hemispheric imbalance using imaging and non-invasive brain stimulation in patients with chronic stroke. *Arch Phys Med Rehabil* 2014;96(4 Suppl):S94–103.
58. Stinear CM, Barber PA, Smale PR, et al. Functional potential in chronic stroke patients depends on corticospinal tract integrity. *Brain* 2007;130(Pt 1):170–80.
59. Schulz R, Park CH, Boudrias MH, et al. Assessing the integrity of corticospinal pathways from primary and secondary cortical motor areas after stroke. *Stroke* 2012;43(8):2248–51.
60. Nouri S, Cramer SC. Anatomy and physiology predict response to motor cortex stimulation after stroke. *Neurology* 2011;77(11):1076–83.
61. Biernaskie J, Szymanska A, Windle V, et al. Bi-hemispheric contribution to functional motor recovery of the affected forelimb following focal ischemic brain injury in rats. *Eur J Neurosci* 2005;21(4):989–99.
62. Fisher CM. Concerning the mechanism of recovery in stroke hemiplegia. *Can J Neurol Sci* 1992;19(1):57–63.

63. Cramer SC, Nelles G, Benson RR, et al. A functional MRI study of subjects recovered from hemiparetic stroke. *Stroke* 1997;28(12):2518–27.
64. Johansen-Berg H, Rushworth MF, Bogdanovic MD, et al. The role of ipsilateral premotor cortex in hand movement after stroke. *Proc Natl Acad Sci U S A* 2002;99(22):14518–23.
65. Machado AG, Shoji A, Ballester G, et al. Mapping of the rat's motor area after hemispherectomy: the hemispheres as potentially independent motor brains. *Epilepsia* 2003;44(4):500–6.
66. Carmel JB, Kimura H, Martin JH. Electrical stimulation of motor cortex in the uninjured hemisphere after chronic unilateral injury promotes recovery of skilled locomotion through ipsilateral control. *J Neurosci* 2014;34(2):462–6.
67. Bachmann LC, Lindau NT, Felder P, et al. Sprouting of brainstem-spinal tracts in response to unilateral motor cortex stroke in mice. *J Neurosci* 2014;34(9):3378–89.
68. Ackerley SJ, Stinear CM, Barber PA, et al. Combining theta burst stimulation with training after subcortical stroke. *Stroke* 2010;41(7):1568–72.
69. Stinear JW, Byblow WD. Rhythmic bilateral movement training modulates corticomotor excitability and enhances upper limb motricity poststroke: a pilot study. *J Clin Neurophysiol* 2004;21(2):124–31.
70. Byblow WD, Stinear CM, Smith MC, et al. Mirror symmetric bimanual movement priming can increase corticomotor excitability and enhance motor learning. *PLoS One* 2012;7(3):e33882.
71. Kloppel S, van Eimeren T, Glauche V, et al. The effect of handedness on cortical motor activation during simple bilateral movements. *Neuroimage* 2007;34(1):274–80.
72. Aramaki Y, Honda M, Sadato N. Suppression of the non-dominant motor cortex during bimanual symmetric finger movement: a functional magnetic resonance imaging study. *Neuroscience* 2006;141(4):2147–53.
73. Grefkes C, Eickhoff SB, Nowak DA, et al. Dynamic intra- and interhemispheric interactions during unilateral and bilateral hand movements assessed with fMRI and DCM. *Neuroimage* 2008;41(4):1382–94.
74. Maki Y, Wong KF, Sugiura M, et al. Asymmetric control mechanisms of bimanual coordination: an application of directed connectivity analysis to kinematic and functional MRI data. *Neuroimage* 2008;42(4):1295–304.
75. Liuzzi G, Horniss V, Zimerman M, et al. Coordination of uncoupled bimanual movements by strictly timed interhemispheric connectivity. *J Neurosci* 2011;31(25):9111–7.
76. Stinear JW, Byblow WD. Disinhibition in the human motor cortex is enhanced by synchronous upper limb movements. *J Physiol* 2002;543(Pt 1):307–16.
77. Ward N. Assessment of cortical reorganisation for hand function after stroke. *J Physiol* 2011;589(Pt 23):5625–32.
78. Ward NS, Brown MM, Thompson AJ, et al. Neural correlates of outcome after stroke: a cross-sectional fMRI study. *Brain* 2003;126(Pt 6):1430–48.
79. Staines WR, McIlroy WE, Graham SJ, et al. Bilateral movement enhances ipsilesional cortical activity in acute stroke: a pilot functional MRI study. *Neurology* 2001;56(3):401–4.
80. Nelles G, Cramer SC, Schaechter JD, et al. Quantitative assessment of mirror movements after stroke. *Stroke* 1998;29(6):1182–7.
81. Dum RP, Strick PL. The origin of corticospinal projections from the premotor areas in the frontal lobe. *J Neurosci* 1991;11(3):667–89.
82. Bradnam LV, Stinear CM, Byblow WD. Ipsilateral motor pathways after stroke: implications for non-invasive brain stimulation. *Front Hum Neurosci* 2013;7:184.

83. Netz J, Lammers T, Homberg V. Reorganization of motor output in the non-affected hemisphere after stroke. *Brain* 1997;120(Pt 9):1579–86.
84. Talelli P, Greenwood RJ, Rothwell JC. Exploring theta burst stimulation as an intervention to improve motor recovery in chronic stroke. *Clin Neurophysiol* 2007;118(2):333–42.